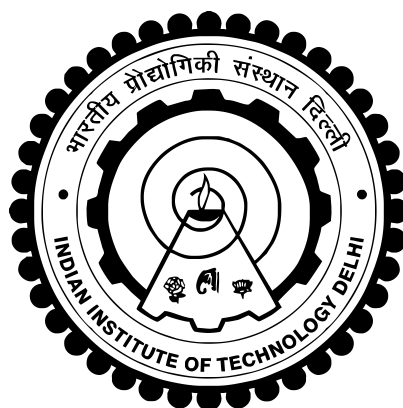


**SOME STUDIES ON A GENERALIZED FOURIER
EXPANSION FOR NONLINEAR AND
NONSTATIONARY TIME SERIES ANALYSIS**

PUSHPENDRA SINGH



**DEPARTMENT OF ELECTRICAL ENGINEERING
INDIAN INSTITUTE OF TECHNOLOGY DELHI**

AUGUST 2016

**SOME STUDIES ON A GENERALIZED FOURIER
EXPANSION FOR NONLINEAR AND
NONSTATIONARY TIME SERIES ANALYSIS**

by

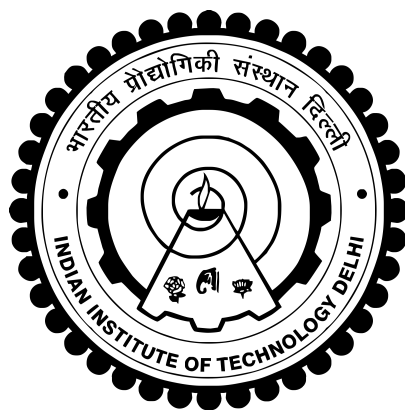
PUSHPENDRA SINGH

DEPARTMENT OF ELECTRICAL ENGINEERING

Submitted

in fulfillment of the requirements of the degree of Doctor of Philosophy

to the



INDIAN INSTITUTE OF TECHNOLOGY DELHI

AUGUST 2016

Dedicated to
MY TEACHERS

&

PARENTS

Smt. Ramlali Singh

Late Shri Shivadhar Singh

Certificate

This is to certify that the thesis entitled “**Some studies on a generalized Fourier expansion for nonlinear and nonstationary time series analysis**” being submitted by **Mr. Pushpendra Singh** to the **Department of Electrical Engineering, Indian Institute of Technology Delhi**, for the award of the degree of **Doctor of Philosophy** is the record of the bona-fide research work carried out by him under our supervision. In our opinion, the thesis has reached the standards fulfilling the requirements of the regulations relating to the degree.

The results contained in this thesis have not been submitted either in part or in full to any other university or institute for the award of any degree or diploma.

(Dr. Shiv Dutt Joshi)

Professor

Department of Electrical Engineering

Indian Institute of Technology Delhi

(Dr. R. K. Patney)

Professor

Department of Electrical Engineering

Indian Institute of Technology Delhi

(Dr. Kaushik Saha)

Director

Samsung R&D Institute India–Delhi

Acknowledgements

First and foremost, I would like to express my deep sense of gratitude and indebtedness to my supervisors Prof. S. D. Joshi, Prof. R. K. Patney and Dr. Kaushik Saha for giving me an opportunity to work under their supervision and guidance. Their excellent supervision, skilled guidance, unfailing support, stimulating discussions and constant encouragement during this thesis work has been invaluable to me. I enjoyed the freedom that I was given during the course of this research work, that allowed me to explore and learn more than I otherwise might have. Their willingness to listen to my presentations and their patient approach to rectifying the mistakes and suggesting improvisations have been the main factors that helped shape this thesis.

This thesis could not be completed without the support of my wife Shraddha Singh. Her invaluable companionship, warmth, strong faith in my capabilities and me, has always helped me to be more assertive at work. Her support, optimistic and enlightening discussions, encouragement, love and extraordinary patience have made it possible to complete this research work.

My sincere thanks to all my friends for their cooperation and providing me very healthy company throughout my research work at IIT Delhi. Their valuable suggestions and criticisms have made me to take right decisions at times. I am especially thankful to Pankaj Kumar Srivastava, Akhilesh Kumar Singh, Amit Srivastava, Suneet Kumar Awasthi, Sanjeev, Vivek Singh, Kapil Dev Tyagi, Amit Singhal, Satyendra Kumar, B. Suresh and Anup Mandpura who have always been at my side even before I called out for any sort of help.

I express my deep sense of reverence and profound gratitude to my parents and family members for their unconditional love and support. I owe all my achievements to them. I

thank my family members Vijay Bahadur Singh, Saroj Singh, Krishna Pal Singh, Vimlesh Singh, Jay Prakash, Avinesh, Arunesh, Priyanka, daughter Prisha and son Siddharth, for their constant support, encouragement, love and exhibiting extra ordinary patience throughout this research work. I am very thankful to my parents-in-law Smt. Bela Patel and Shri K.L. Patel for their love, continuous support and blessings. I also express my sincere thanks to my brothers-in-law and sisters-in-law for their progressive discussions, motivations and healthy company.

I gratefully acknowledge the guidance, discussions and support provided in numerous ways by Prof. Hariom Gupta, director, IIIT Noida.

Pushpendra Singh

Abstract

The main objective of this thesis is to investigate and develop adaptive signal decomposition methods that yield a set of basis vectors, which are complete, orthogonal, local and adaptive. The instantaneous frequencies and square of amplitudes of these basis vectors produce a Time-Frequency-Energy (TFE) distribution, referred to as the Hilbert spectrum, that reveals the embedded structures of a signal. The main results of this thesis are briefly described in the following.

As is well known the Empirical Mode Decomposition (EMD) algorithm provides a general method for examining the TFE distribution of nonlinear and nonstationary time series. One of the important steps, in the EMD, is to obtain upper and lower envelopes by cubic spline interpolation of local extrema (maxima and minima) of a time series. Hence it is obvious that the performance of the algorithm would depend upon the type of interpolation and the locations of extrema in a time series. Deeper investigation leads to a novel nonpolynomial spline based EMD that reduces mode mixing and detrend uncertainty, which are some shortcomings of the EMD algorithm in the analysis of time series. A number of results on nonpolynomial interpolation, approximation and concomitant error analysis are presented. The generalized error analysis results for nonpolynomial, Hermite nonpolynomial interpolations and Taylor's nonpolynomial series approximation are derived. The EMD presented here improves the orthogonality among Intrinsic Mode Functions (IMFs) but does not make them completely orthogonal, therefore, energy is not preserved in the decomposition and there is always some energy leakage among IMFs.

We next propose algorithms which preserve energy in EMD. In the first Energy Preserving EMD (EPEMD) algorithm, a signal is decomposed into Linearly Independent (LI), Non Orthogonal yet Energy Preserving (LINOEP) IMFs and the residue. It is shown that

a vector in an inner product space can be represented as a sum of LI but non orthogonal vectors in such a way that Parseval's equality type property is satisfied. We first observe that from the set of ' n ' IMFs, via the Gram-Schmidt Orthogonalization Method (GSOM), $n!$ sets of orthogonal functions can be obtained. In the second algorithm, we show that if the orthogonalization process proceeds from the lowest frequency IMF to the highest frequency IMF, then the GSOM yields functions which preserve the properties of IMFs and energy of the signal. However, all EMD algorithms are empirical in nature and do not provide a complete mathematical foundation required to fully understand the EMD. This motivates us to further explore and develop methods that capture all the relevant features and are also based on some sound mathematical foundation.

For many decades, there is a general perception in the literature that Fourier methods are not suitable for the analysis of nonlinear and nonstationary time series. We propose such a mathematical foundation in the form of a Fourier Decomposition Method (FDM) and demonstrate its efficacy for the analysis of nonlinear and nonstationary time series. The proposed FDM decomposes any data into a small number of 'Fourier Intrinsic Band Functions' (FIBFs). The FDM presents a generalized Fourier expansion with variable amplitudes and frequencies of a time series by the Fourier method itself. We also propose an idea of the zero-phase filter bank based Multivariate FDM (MFDM) algorithm for analysis of multivariate nonlinear and nonstationary time series. We also present an algorithm to obtain cutoff frequencies of zero-phase filter bank for MFDM.

Finally, we present a Fourier base method for the analysis and classification of electroencephalogram (EEG) signals using EEG rhythms. This method is based on MFMD method that analyzes common frequency components in multichannel EEG recordings. The Mean Frequency (MF) and RMS bandwidth are estimated from the EEG rhythms which are found to be statistically different, for the different classes of EEG recordings, and hence used to distinguish and classify the two classes of signals using a least-squares support vector machine (LS-SVM) classifier. Experimental results on a publicly available database demonstrate that the proposed feature sets effectively characterize the EEG rhythms and are suitable for classification between different classes of EEG signals.

Contents

Certificate	i
Acknowledgements	iii
Abstract	v
List of Figures	xi
List of Tables	xxi
List of abbreviations and symbols	xxiii
1 Issues in Nonlinear and Nonstationary Time Series Analysis	1
1.1 Introduction	1
1.2 Brief literature survey	4
1.2.1 Instantaneous frequency	4
1.2.2 The spectrogram	8
1.2.3 The Wigner-Ville distribution	9
1.2.4 Wavelet analysis	11
1.2.5 Evolutionary spectrum	12
1.2.6 The empirical mode decomposition	12
1.2.7 Other miscellaneous methods	14
1.3 Motivation and scope of the thesis	14
1.4 Salient contributions	17
1.5 Overview of the thesis	18

2	Preliminaries	23
2.1	Introduction	23
2.2	Stationary and nonstationary processes	23
2.3	Time-invariant, linear and nonlinear systems	24
2.4	The empirical mode decomposition algorithms	26
2.5	Uncertainty principle	31
2.6	The Hilbert spectrum	32
2.7	Conclusions	34
3	A Novel Nonpolynomial Interpolation Scheme: Theory, Error Analysis and Application to EMD	35
3.1	Introduction	35
3.2	Nonpolynomial spline interpolation	38
3.2.1	The nonpolynomial cubic spline interpolation	40
3.2.2	The Hermite nonpolynomial cubic spline interpolation	42
3.3	The Taylor's nonpolynomial series approximation	43
3.4	Nonpolynomial, polynomial interpolation and the Fourier series represen- tation	44
3.5	Error analysis results	45
3.5.1	The error analysis in the Taylor's nonpolynomial series approximation	45
3.5.2	The error analysis in nonpolynomial interpolation	46
3.6	Nonpolynomial spline based empirical mode decomposition	49
3.7	Simulations and numerical results	51
3.7.1	Error in spline interpolation	51
3.7.2	Error in Taylor's nonpolynomial approximation	56
3.7.3	Application of nonpolynomial cubic spline interpolation in EMD algorithm	60
3.8	Conclusions	67
4	The Hilbert Spectrum and Energy Preserving Empirical Mode Decom-	

position	69
4.1 Introduction	69
4.2 Preliminaries: The GSOM and orthogonal EMD	70
4.3 EPEMD: Nonorthogonal approach	72
4.4 EPEMD: Orthogonal approach	75
4.5 Simulations and numerical results	79
4.5.1 A Comparison of energy leakage between the EMD and EPEMD . .	79
4.5.2 Real life time series decomposition	80
4.5.3 A comparison of percentage energy error (Pee) between the MEMD and OMEMD	83
4.5.4 The time-frequency analysis of chirp signal	84
4.5.5 The statistical significance of IMFs generated by the proposed EPEMD algorithms	86
4.6 Conclusions	90
5 The Fourier Decomposition Method for Nonlinear and Nonstationary Time Series Analysis	95
5.1 Introduction	95
5.2 The Fourier decomposition method	97
5.2.1 Continuous Time FDM (CT-FDM)	98
5.2.2 Discrete Time FDM (DT-FDM)	101
5.3 Multivariate Fourier decomposition method	104
5.4 The FDM for continuous time real function	107
5.5 The FDM for discrete time real function	109
5.6 Simulation and numerical results	111
5.6.1 Intermittency and mode mixing	111
5.6.2 Multivariate data decomposition	111
5.6.3 TFE analysis of mixture of linear chirp and FM sinusoid	113
5.6.4 Intrawave frequency modulation	113
5.6.5 Analysis of a white Gaussian noise	117

5.6.6	TFE analysis of unit sample sequence	120
5.6.7	Application to a earthquake signal analysis	121
5.6.8	Application to a speech signal analysis	123
5.7	Conclusions	125
6	Fourier-Based Feature Extraction for Classification of EEG Signals Using EEG Rhythms	131
6.1	Introduction	131
6.2	Preliminaries: Least-squares support vector machine	134
6.3	Filter bank approach for the decomposition and extraction of mean frequencies and RMS bandwidths	137
6.4	Simulation results and discussion	140
6.5	Conclusions	148
7	Conclusions and Scope for Future Work	151
7.1	Introduction	151
7.2	Summary of results	151
7.3	Scope for further work	155
	References	157
A	Appendix: LINOEP vectors	171
A.1	Introduction	171
A.2	A general algorithm to obtain LINOEP vectors	171
A.3	The LINOEP method	172
A.4	Many solutions to preserve the square of norm	174
	List of Publications	177
	Biography of Pushpendra Singh	179

List of Figures

3.1	MAE (with L_∞ Norm minimization) in polynomial cubic spline (PolyCubicSpline) and nonpolynomial cubic spline (NonPolyCubicSpline) interpolation of signal $x_k(t_i)$ in Example 1, with Boundary Condition (BC) Not a Knot (NaK), BC Clamped (BCC) and BC Natural (BCN)	52
3.2	MAE (with L_1 Norm minimization) in polynomial and nonpolynomial cubic spline interpolation of signal $x_k(t_i)$ in Example 1, with Boundary Condition (BC) Not a Knot (NaK), BC Clamped (BCC) and BC Natural (BCN). . .	53
3.3	MAE (with L_2 Norm minimization) in polynomial and nonpolynomial cubic spline interpolation of signal $x_k(t_i)$ in Example 1, with Boundary Condition (BC) Not a Knot (NaK), BC Clamped (BCC) and BC Natural (BCN). . .	54
3.4	MAE (with L_∞ -norm minimization) in polynomial and nonpolynomial cubic spline interpolation of signal $f(t_i)$ in Example 2, with Boundary Condition (BC) Not a Knot (NaK), BC Clamped (BCC) and BC Natural (BCN). . .	55
3.5	MAE (with L_∞ -norm minimization) in nonpolynomial interpolation of signal $f(t_i)$ in Example 2.	56
3.6	MAE (with L_∞ -norm minimization) in Hermite nonpolynomial cubic spline (NonPolyCubicSpline) interpolation of signal $x_k(t_i)$ in Example 3 with $\tau = 3$ (top one), $\tau = 1$ (middle one) and $\tau = 0.25$ (bottom one).	57
3.7	Absolute error in the Taylor's polynomial and nonpolynomial (with L_∞ -norm minimization $\omega_1 = 0.69$) approximation of $y(t)$ in Example 4.	58

3.8	Top and middle plots are absolute errors (AE) and corresponding parameters (ω) plots, bottom plot is AE plot with single parameter ($\omega = -3.29$) in the Taylor's polynomial and nonpolynomial approximation of $f(t)$ in Example 5 with L_∞ -norm minimization.	60
3.9	The annual mean global surface temperature anomaly	61
3.10	A set of IMFs obtained from EMD with PCS.	62
3.11	A set of IMFs obtained from EMD with NPCS.	62
3.12	Time series $x(t)$, containing a high frequency $x_1(t)$, and low frequency $x_2(t)$, and component without trend $x_3(t)$	63
3.13	Proposed EMD analysis of time series $x(t)$ given in Fig. 3.12, IMFs $y_1(t)$, $y_2(t)$, $y_3(t)$ resemble the $x_1(t)$, $x_2(t)$, $x_3(t)$ components, respectively. It clearly shows the capability of mode mixing and detrend uncertainty. . . .	63
3.14	Time series $x(t)$ and its components $x_1(t)$, $x_2(t)$, $x_3(t)$, and $x_0(t)$	64
3.15	Proposed EMD analysis of time series $x(t)$ given in Fig. 3.14, IMFs $y_1(t)$, $y_2(t)$, $y_3(t)$, $y_0(t)$ resemble the $x_1(t)$, $x_2(t)$, $x_3(t)$, $x_0(t)$ components, respectively. It clearly shows the capability of trend determination.	65
3.16	Detrend of three noisy signals $s_1(t_i)$, $s_2(t_i)$, and $s_3(t_i)$ by proposed EMD. Here dashed-dashed curve is the trend of the signal, and solid curve is the trend determined using the proposed EMD algorithm.	66
3.17	Time series $x(t)$ and its components $x_1(t)$, $x_2(t)$, $x_3(t)$, and noise $n(t)$	67
3.18	Proposed EMD analysis of time series $x(t)$ given in Fig. 3.17, IMFs $y_4(t)$, $y_5(t)$, and trend $y_6(t)$ resemble the components $x_1(t)$, $x_2(t)$, and trend $x_3(t)$, respectively. It clearly shows the capability of trend determination and mode mixing elimination in presence of noise.	67
4.1	Three non orthogonal vectors $\mathbf{c}_1, \mathbf{c}_2, \mathbf{c}_3$ such that $\mathbf{c}_1 \perp (\mathbf{c}_2 + \mathbf{c}_3)$, $\mathbf{c}_2 \perp \mathbf{c}_3$ and vector $\mathbf{x} = \mathbf{c}_1 + \mathbf{c}_2 + \mathbf{c}_3$ in 3-D.	76
4.2	Linearly Independent (LI) vectors can be Orthogonal (O), Uncorrelated (U), Orthogonal and Uncorrelated (O&U) in an inner product space. . . .	76

4.3	Over all Index of Orthogonality (IO_T) for different types of signal. Values of IO_T with EPEMD is always in the range of 10^{-15} which is almost zero (ideal value), whereas there is a large variations (peak value of $IO_T \approx -1.6$) in value of IO_T with EMD.	80
4.4	Comparison between EMD and EPEMD by over all Index of Orthogonality (IO_T) with different sampling frequency (100 to 400 Hz). Values of IO_T with EPEMD is always in the range of 10^{-15} which is almost zero (ideal value), whereas there is a large variations in value of IO_T with EMD (peak value of $IO_T \approx -58$).	80
4.5	Comparison between EMD and EPEMD by over all Index of Orthogonality (IO_T) with different sampling frequency (100 to 2000 Hz). Values of IO_T with EPEMD is always in the range of 10^{-15} which is almost zero (ideal value), whereas there is a large variations in value of IO_T with EMD (peak value of $IO_T \approx -11.5$).	81
4.6	Annual mean global surface temperature anomaly data.	83
4.7	Set of IMFs (top to bottom) y_1 to y_4 and $(y_5 + y_6 + r_6)$ obtained from EMD.	84
4.8	Set of FOIMFs (top to bottom) y_1 to y_4 and $(y_5 + y_6 + r_6)$ obtained from EMD. Clearly, there is mode mixing problem, that is, high frequency components are mixed in low frequency ones.	84
4.9	Set of ROIMFs (top to bottom) y_1 to y_4 and $(y_5 + y_6 + r_6)$ obtained from proposed EMD. There is no mode mixing problem.	85
4.10	Set of ROUIMFs (top to bottom) y_1 to y_4 and $(y_5 + y_6 + r_6)$ plus DC component obtained from proposed EMD. There is no mode mixing problem.	85
4.11	Set of IMFs (top to bottom) y_1 to y_4 and $(y_5 + y_6 + r_6)$ obtained from EEMD.	86
4.12	Set of FOIMFs (top to bottom) y_1 to y_4 and $(y_5 + y_6 + r_6)$ obtained from EEMD. Clearly, there is mode mixing problem, that is, high frequency components are mixed in low frequency ones.	86

4.13	Set of ROIMFs (top to bottom) y_1 to y_4 and $(y_5 + y_6 + r_6)$ obtained from proposed EEMD. There is no mode mixing problem and energy of signal is preserved in decomposition.	87
4.14	Set of ROUIMFs (top to bottom) y_1 to y_4 and $(y_5 + y_6 + r_6)$ plus DC component obtained from proposed EEMD. There is no mode mixing problem and energy of signal is preserved in decomposition.	87
4.15	Elcentro Earthquake May 18, 1940 North-South Component	88
4.16	Hilbert marginal spectrum for Elcentro Earthquake May 18, 1940 North-South component time series with (top to bottom) IMFs, FOUIMFs, ROUIMFs and EPIMFs.	88
4.17	4-variate signal $x_j(t)$ (first row) and its IMFs (second row onwards) obtained from MEMD, by equation (4.15), in each column, where x-axis represents time and y-axis represents amplitude.	89
4.18	Set of FOIMFs obtained from MEMD by equation (4.15), where x-axis represents time and y-axis represents amplitude. Clearly, there is mode mixing problem, that is, high frequency components are mixed in low frequency ones.	89
4.19	Set of ROIMFs obtained from proposed MEMD by equation (4.15), where x-axis represents time and y-axis represents amplitude. There is no mode mixing problem and energy of signal is preserved in decomposition.	90
4.20	Time-Frequency Analysis of linear chirp with zero padding by (top to bottom) EMD, EEMD and proposed EPEDM. Clearly, proposed method outperforms other ones.	90
4.21	Significance test of the IMFs of the Gaussian white noise. The EMD generates two IMF components, outside of upper and lower bound, which are spurious.	91
4.22	Significance test of the EPIMFs of the Gaussian white noise. The proposed EMD generates no spurious components.	91

4.23	Significance test of the FOIMFs of the Gaussian white noise. The EMD generates eleven IMF components, outside of upper and lower bound, which are spurious.	92
4.24	Significance test of the ROIMFs of the Gaussian white noise. The proposed EMD generates no spurious components.	93
4.25	Significance test of the ROUIMFs of the Gaussian white noise. The proposed EMD generates no spurious components.	93
5.1	Decompositions of a signal $x(t)$ (a) which is a sinusoid mixed with intermittent interference through algorithm of (b) proposed FDM (c) EMD and (d) EEMD.	112
5.2	MFDM applied to a quadri-variate tone-noise mixture (top row), generates perfectly aligned intrinsic modes in all the four channels (fourth to seventh row), and second and third row contain the noise components.	113
5.3	The TFE analysis of nonstationary signals which is mixture of linear chirp and FM sinusoid: FDM (top and middle) and EMD (bottom).	114
5.4	The signal $x(t)$ (solid line), sum of mean-value and lowest frequency FIBF (dashed line) of (5.44).	115
5.5	The mean-value, FIBF1, FIBF2 and highest frequency component by FDM (top to bottom). The mean-value and highest frequency component correspond to term $X[0]$ and $X[\frac{N}{2}](-1)^n$ of (5.15), respectively. Sum of mean-value, FIBF1, FIBF2 and highest frequency component exactly synthesize signal $x(t)$ given by (5.44).	115
5.6	The TFE analysis of signal $x(t)$ given by (5.44): FDM (top) and EMD (bottom). Notice end effect artefacts in TFE plot by EMD.	116
5.7	The TFE analysis of signal $x(t)$ given by (5.45): FDM (top) and EMD (bottom). Notice end effect artefacts in TFE plot by EMD.	117

5.8	The TFE analysis of the Gaussian white noise (with zero mean and unit variance): FDM (top and middle) and EMD (bottom). The FDM is able to decompose data into distinct frequency bands, whereas bands are not clearly separated by EMD.	118
5.9	The PSD analysis of the Gaussian white noise (with zero mean and unit variance): FDM (top and middle) and EMD (bottom). The FDM is able to decompose data into distinct frequency bands, whereas bands are not clearly separated by EMD.	119
5.10	The analytic representation of $\delta[n-n_0]$ (with, $n_0 = 199$, sampling frequency $F_s = 100$ Hz, length $N = 400$): Real part of $z[n]$ (top), Imaginary part of $z[n]$ (middle) and absolute value of $z[n]$ (bottom).	120
5.11	The TFE analysis of unit sample sequence $\delta[n - n_0]$ (with, $n_0 = 199$, sampling frequency $F_s = 100$ Hz, length $N = 400$) by the: FDM (top), EEMD (middle) and continuous wavelet transform (CWT) (bottom). The energy is concentrated in both time and frequency in TFE plot by the FDM (that is, it is not limited by uncertainty principle), whereas there is spreading of the energy in TFE plots by EEMD and CWT.	122
5.12	The mean-value, FIBF1, FIBF2 and highest frequency component plots by the FDM of unit sample sequence $\delta[n - n_0]$ (with, $n_0 = 199$, sampling frequency $F_s = 100$ Hz, length $N = 400$).	123
5.13	Plot of (top to bottom): (a) Elcentro Earthquake May 18, 1940 North-South Component, (b) Fourier based power spectral density (PSD).	124
5.14	Plot of (top to bottom): (a) Marginal spectrum by FDM, (b) Marginal spectrum by EMD.	125
5.15	Plot of the instantaneous energy density $E(t)$ (top to bottom) using the: (a) FDM and (b) EMD.	126
5.16	Plot of TFE (top to bottom) using the: (a) FDM (b) EMD and (c) CWT.	127

5.17	Vowel ‘small-cap I’ sound with sampling frequency $F_s = 16000$ Hz (top left) and its Fourier spectrum (top right). The FDM generates highest frequency component (y_1), FIBFs (y_2 to y_{11}) and mean-value component (y_{12}). The fundamental frequency F_0 is captured accurately in FIBF y_8 . . .	128
5.18	IMFs (y_1 to y_{12}) generated by (a) EMD and (b) EEMD (with zero mean and 0.2 standard deviation of the added noise of normal distribution and the ensemble size of 300) algorithms for vowel ‘small-cap I’ with $F_s = 16000$ Hz. The EMD is not able to catch F_0 in any mode, and the EEMD is able to capture F_0 accurately in IMF y_5	129
5.19	The TFE plot by FDM (top) EMD (middle) and (b) EEMD of same data (vowel ‘small-cap I’). There is enhanced TFE tracking when using FDM and it captures F_0 accurately in voice signal.	130
6.1	Frequency response of filter bank with cutoff frequencies, based on the EEG rhythms, $f_{c1} = 30$ Hz, $f_{c2} = 13$ Hz, $f_{c3} = 8$ Hz, $f_{c4} = 4$ Hz, and sampling frequency $f_s = 173.61$ Hz.	137
6.2	Block diagram of the FFT based filter bank, MF and RBW estimation and classification method: input EEG signals $x_\ell[n]$, output IBFs $y_{\ell p}[n]$, estimate upper envelopes of IBFs and remove mean to obtain $u_{\ell p}[n]$, the MF $\mu_{\ell p}$ and RBW $\sigma_{\ell p}$, LS-SVM classifier, class 1 and class 2 outputs. . . .	139
6.3	Intrinsic Band functions of the 23.6 seconds seizure-free (top $x_\ell[n]$) and seizure (bottom $x_\ell[n]$) EEG signals. The ℓ th channel EEG signal $x_\ell[n]$ (both top and bottom) is exact sum of the orthogonal components $y_{\ell 1}[n]$ (γ wave: 30–70 Hz), $y_{\ell 2}[n]$ (β wave: 13–30 Hz), $y_{\ell 3}[n]$ (α wave: 8–13 Hz), $y_{\ell 4}[n]$ (θ wave: 4–8 Hz), $y_{\ell 5}[n]$ (δ wave: 0.1–4 Hz) and $y_{\ell 6}[n]$ (residue: <0.1 Hz).	141

6.4	Comparison of values of MF calculated for EEG signals (A, B, C, D and E) using the Kruskal–Wallis test. The subplot shows the comparison of MF estimates (I_μ) among the γ (> 30 Hz), β (13–30 Hz), α (8–13 Hz), θ (4–8 Hz) and δ (0.1–4 Hz) waves (top to bottom) of data sets, and p values are [113.4097e-066, 9.7554e-021, 33.1426e-057, 70.2678e-027, 37.0251e-048], respectively.	143
6.5	Comparison of values of RBW calculated for EEG signals (A, B, C, D and E) using the Kruskal–Wallis test. The subplot shows the comparison of RBW estimates (I_σ) among the γ (> 30 Hz), β (13–30 Hz), α (8–13 Hz), θ (4–8 Hz) and δ (0.1–4 Hz) waves (top to bottom) of data sets, and p values are [124.6074e-066, 55.8299e-027, 882.1086e-021, 3.1267e-006, 72.2970e-009], respectively.	143
6.6	Comparison of values of MF calculated for EEG signals (A, B, C, D and E) using the Kruskal–Wallis test. The subplot shows the comparison of MF estimates of envelopes (E_μ) among the γ (> 30 Hz), β (13–30 Hz), α (8–13 Hz), θ (4–8 Hz) and δ (0.1–4 Hz) waves (top to bottom) of data sets, and p values are [13.4737e-051 230.2043e-027 26.7942e-024 55.8459e-003 48.9730e-006], respectively.	144
6.7	Comparison of values of RBW calculated for EEG signals (A, B, C, D and E) using the Kruskal–Wallis test. The subplot shows the comparison of RBW estimates of envelopes (E_σ) among the γ (> 30 Hz), β (13–30 Hz), α (8–13 Hz), θ (4–8 Hz) and δ (0.1–4 Hz) waves (top to bottom) of data sets, and p values are [841.0928e-066, 12.6771e-009, 284.2688e-051, 1.7820e-018, 161.7435e-027], respectively.	144
6.8	The ROC curve plots with polynomial, RBF and linear kernel function of LS-SVM classifier for classification between set A and E with 20 features of EEG signals.	145

6.9	Classification between set A and E signal classes using the LS-SVM classifier with RBF kernel (top) and corresponding ROC plot (bottom) with 2 features (I_μ and I_σ) of first IBF of EEG signals.	146
A.1	Three non orthogonal vectors c_1, c_2, c_3 such that $c_1 \perp (c_2 + c_3)$ and vector $s = c_1 + c_2 + c_3$ in 3-D.	175
A.2	Three non orthogonal vectors c_1, c_2, c_3 such that $\langle \mathbf{c}_2, \mathbf{c}_3 \rangle + \langle \mathbf{c}_1, \mathbf{c}_2 \rangle = -\langle \mathbf{c}_1, \mathbf{c}_3 \rangle$ and vector $s = c_1 + c_2 + c_3$ in 3-D.	176

List of Tables

3.1	Comparison of MAE among PCS, NPCS and HNPCS for signals of Fig. 3.1 with Not a Knot BC. S*:Signals, a*:MAE in PCS, b*:MAE in NPCS, and c*:MAE in HNPCS.	51
3.2	Comparison between IMFs with PCS (IMFs_PCS) and IMFs with NPCS (IMFs_NPCS) for signals of Fig. 3.9 with Not a Knot BC. Energy of signal $E = 11.3752$ and E_6^* is energy of residue component. E*:Energy, f*:IMFs_PCS, g*:IMFs_NPCS.	61
3.3	PCC and RRMSE between $x_k(t)$ and $y_k(t)$	64
4.1	Comparison between EMD and EPemd by over all index of orthogonality (IO_T).	82
4.2	The signal energy $E_x = 11.3752$, components and sum of components energies and Pee for IMFs, OIMFs, FOIMFs and ROIMFs obtained from EMD. E_7^* is energy of residue component.	82
4.3	Percentage error in energy (Pee) for IMFs, OIMFs, and ROIMFs obtained from EMD for Elcentro Earthquake data.	82
4.4	Pee for IMFs, FOIMFs and ROIMFs obtained from MEMD	83
5.1	Comparisons among Fourier, Wavelet, EMD-Hilbert and FDM methods in data analysis.	110
6.1	p-Values of MF and RMS bandwidth (RBW) estimates among EEG signals (A, B, C, D and E) for IBF1 to IBF5 using the Kruskal–Wallis test. . . .	142

6.2	A measure of overall performance of the LS-SVM classifier by estimating area under the ROC curve (AUC) for all possible combination of two sets of EEG signals (A, B, C, D and E), AB versus CD and ABCD versus E with 20 features for (a) polynomial kernel (b) RBF kernel and (c) linear kernel. Here, xx–xx denotes case xx versus xx and xx can be any one of 8 cases A, B, C, D, E, AB, CD and ABCD.	142
6.3	A Comparison of classification accuracy obtained by proposed method and other methods for EEG classification problems (cases).	147

List of abbreviations and symbols

FS	Fourier Series
FT	Fourier Transform
STFT	Short-Time Fourier Transform
TF	Time–Frequency
IF	Instantaneous Frequency
FM	Frequency Modulation
AM	Amplitude Modulation
HT	Hilbert Transform
WVD	Wigner–Ville Distribution
CWT	Continuous Wavelet Transform
TFE	Time-Frequency-Energy
TFD	Time-Frequency Distribution
TFR	Time-Frequency Representation
FFT	Fast Fourier Transform
PCS	Polynomial Cubic Spline
NPCS	Nonpolynomial Cubic Spline
HNPCS	Hermite Nonpolynomial Cubic Spline
EMD	Empirical Mode Decomposition

EEMD	Ensemble EMD
MEMD	Multivariate EMD
MEMD	Orthogonal Multivariate EMD (OMEMD)
OEMD	Orthogonal EMD
EPEMD	Energy Preserving EMD
IMF	Intrinsic Mode Function
MIMF	Multivariate IMF
EPIMF	Energy Preserving IMF
FOIMF	Forward Orthogonal Intrinsic Mode Function
ROIMF	Revere Orthogonal Intrinsic Mode Function
ROUIMF	Revere Orthogonal and Uncorrelated Intrinsic Mode Function
DFT	Discrete Fourier Transform
IDFT	Inverse Discrete Fourier Transform
LINOEP	Linearly Independent Non Orthogonal yet Energy Preserving
GSOM	Gram-Schmidt Orthogonalization Method
FDM	Fourier Decomposition Method
FIBF	Fourier Intrinsic Band Function
MFIBF	Multivariate FIBF
MFDM	Multivariate FDM
AFIBF	Analytic FIBF
ZPFB	Zero-phase Filter Bank
FHS	Fourier-Hilbert Spectrum
MF	Mean Frequency

RMS	Root Mean Square.
RBW	Root Mean Square Bandwidth
EEG	Electroencephalography
IBF	Intrinsic Band Function
MIBF	Multivariate IBF
LS-SVM	Least-Squares Support Vector Machine
RBF	Radial Basis Function
ROC	Receiver Operating Characteristic
AUC	Area Under the ROC Curve
DSP	Digital Signal Processing
IIR	Infinite Impulse Response
FIR	Finite Impulse Response
C^∞ function	A C^∞ function (or smooth function) is a function that is differentiable for all degrees of differentiation.
ω	Based on the context, it is the frequency in <i>radians/second</i> and <i>radians/sample</i> for a continuous and discrete time signal, respectively.