

SOME SIGNAL PROCESSING TECHNIQUES FOR ULTRASONIC  
TISSUE CHARACTERISATION

Mahalovya Gauba

Thesis submitted to  
INDIAN INSTITUTE OF TECHNOLOGY  
NEW DELHI

for the award of the degree of

DOCTOR OF PHILOSOPHY

Centre for Biomedical Engineering  
Indian Institute of Technology,  
New Delhi-110016

January, 1984

DEDICATED

TO

MY MOTHER, FATHER AND BROTHER

CERTIFICATE

This is to certify that the thesis entitled  
"Some Signal Processing Techniques for Ultrasonic Tissue  
Characterisation" by Mahalovya Gauba is a record of  
original bonafide research carried out under our supervision  
and has not been submitted elsewhere for a degree.

(B.B. Madan)  
Assistant Professor  
Dept. of Computer Science  
and Engineering  
Indian Institute of Tech.  
New Delhi-16

(S.N. Tandon)  
Professor  
Centre for Biomedical Engg.  
Indian Institute of Technology,  
New Delhi-16

Dated Jan. 19, 1984

ACKNOWLEDGEMENT

The Ph.D. programme which has nearly spanned over five and half years has been full of enrichening experiences. During this period, I went through both good and bad times. I had the pleasure of meeting both helpful and not so helpful people. I do not hold back anything against those who have not been helpful for I am sure they must have had their limitations. But all the same I would like to put it on record my gratitude for all those who with all their sincerity have meant to help me.

Dr. S.N. Tandon and Dr. B.B. Madan, two wonderful people, who besides having supervised my work, have also from time to time shown me the way for a better tomorrow. Dr. Tandon has been instrumental in apprising me the applications and scope of ultrasound in medicine. I am grateful to Dr. Madan for having developed in me an interest for signal processing. This means a lot more in the light of the fact that when I joined him as a student, my knowledge in signal processing was limited to what a sinusoid is.

It was on the invitation of Dr. M.P. Kadaba that I got an opportunity to visit America and work for a year in his lab at Helen Hayes Hospital, New York, U.S.A.. He is a brilliant experimentalist and has been responsible for developing in me a temperament for biological experiments. He has been encouraging all through my stay and is a gem of a man. My thanks also goes to all those wonderful people in Helen Hayes Hospital, who inspite of my pestering, made my stay in America a pleasant and a memorable experience.

Dr. Bhaskar Bhattacharya a noble soul, who left no stones unturned in transforming me into a researcher from some one who had been prepared for the production floor. He has been a terrific friend and I only wish, more of us can have friends like him.

I am thankful to Dr. R.B. Kuc who invited me to visit his lab at Yale University, New Haven, U.S.A. During my visit there which stretched over several hours, I discussed various aspects of the technique proposed by him. He was very open and warm.

I very much appreciate the patient hearings that Dr. Vaikunth Gupta gave to me on the phone when I was trying to implement the technique proposed by him. He has been encouraging all along.

On several occasions I have ventured to barge into Dr. Surinder Prasad's office to discuss certain problems during my thesis writing. He was always willing to help and was very polite.

It was nice of Dr. Nasir Ahmed to accommodate me in his busy schedule, when I rang him up to discuss the algorithm proposed by him.

It was indeed kind of Dr. A.C. Kak for making the digitized data of the basic pulse available to me. Most of the simulative work presented in this thesis has been carried out using this data.

I am grateful to Dr. S.K. Guha for having given me an initial exposure of biomedical engineering which has come very handy in building up my background in this field.

It was indeed considerate of Dr. Harpal Singh for having lent me his office space during my thesis writing. I very much appreciate this thoughtful gesture of his.

I dare not give my colleagues Arun Agarwal, Ashok Mallik, Nirmal Jain, Pradeep Sharma, S.M.K. Rahman, Satpal Singh and Subhash Bhalla, a back seat for they from time to time have cheered me up and have provided a very stimulating company.

My thanks also goes to my dear friends Ashwani Datta, Arvind Jain, Ahmed Cameron, Ashok Gupta, L. Shankar, Rakesh Kumar Jain, Rajneesh Garg and Surinder Bansal who over these years have reminded me every evening, the other side of the life.

I am especially thankful to Mr. Ashwani Gupta and Navneet Jindal, my friends since teens, whose affections and generosity have been making me go all this time.

Lastly I must mention two important persons without whose help this thesis might not have seen the light of the day. Thanks to Mr. N.D. Arora for his careful typing and Mr. N.L. Arora for making the figures presentable.

## ABSTRACT

The interest in ultrasound as a medical diagnostic tool stems from the fact that it is harmless at diagnostic levels and can be non-invasively used. Earlier applications of ultrasound in medical diagnosis were limited to imaging and blood flow measurements. But in the recent past, with medical diagnosis becoming more objective, a general need has been felt to express the tissue state in quantitative terms. This involves the identification of suitable parameters which can quantitatively express the condition of the tissue. The identification and study of the parameters which characterise the ultrasound tissue interaction is referred to as 'ultrasound tissue characterisation'. The present work has identified some of these parameters. The discussion of each of these parameters has been presented as a study in this thesis. Following are the studies which have been conducted.

- A. Applicability of the technique proposed by Kuc for the estimation of attenuation coefficient slope of tissues with small thickness and also discusses some of the applicational aspects of the technique.
- B. Study of the applicability of various deconvolution techniques to the problem of identification of interfaces in the tissue.

C. Feasibility of estimating propagation velocity in tissues with small thickness using unwrapped phase spectrum.

A. Study of Various Applicational Aspects of Kuc's Technique

The study presents a statistical technique proposed by Kuc and Schwartz for the estimation of attenuation coefficient slope of liver tissue, whose thickness typically in adult humans is of the order of 10.0 cms. It then discusses some of the applicational aspects of the technique which till now had been overlooked and they are (i) window length; (ii) window shift; and shape of the window to be used for segmentation. These aspects have been studied using wide ranging signal to noise ratios (SNRs). By means of a hypothetical example, the feasibility of this technique for characterising tissues of the order of 1.5 cms has been discussed. It then finally presents the results for the normal and the pathology induced muscle tissues.

The simulative study undertaken has shown that

- (i) the estimate improves as the total numbers of segment pairs increase;
- (ii) Hanning window gives better performance than the hybrid window; and

- (iii) The technique can be used for estimating attenuation coefficient slope of tissues with small thickness but at the cost of increased computational effort.

The estimates of attenuation coefficient slope obtained from normal and pathology induced muscle tissue have been shown to be statistically different.

B. Deconvolution Techniques for the Identification of Interfaces in the Tissues

The study of localised changes in a tissue involves the detailed investigation of its structure. This can be carried out by identifying and studying those parameters which vary spatially in the tissue. Acoustic impedance (hence forth referred simply as impedance) is one such parameter. The impedance difference between two adjacent regions in the tissue could be both small or large. The large scale impedance differences give rise to interfaces. Identification of spatial locations of these interfaces is one of the tissue characterisation problems.

The problem of identification of interfaces in a tissue has been approached by studying the tissue backscatters. The tissue backscatter can be regarded as the convolution of the unit sample response of the tissue and the input

pulse. The problem then reduces to deconvolution of the unit sample response, which is a sequence of unit samples (reflection sequence). Each unit sample corresponds to the spatial location of the interface in the tissue.

The objective of this study is to investigate the suitability of the existing deconvolution techniques and to develop some new approaches for the purpose of spatial identification of these interfaces. Different types of techniques studied are as follows -

- (i) Frequency Domain Techniques;
- (ii) Homomorphic Filtering;
- (iii) Linear Prediction Techniques; and
- (iv) White Noise Estimator.

#### Frequency Domain Techniques

This includes the application of two standard deconvolution techniques i.e. inverse and Wiener filtering and a more recently proposed approach - 'spectral equalisation'. Spectral equalisation is basically heuristic in nature and involves the compression of overlapping pulses into narrow pulses, which are now easier to resolve.

#### Homomorphic Filtering

Two aspects of homomorphic filtering i.e. complex cepstrum and power cepstrum have been studied. These aspects

are relevant to the underlying convolutional model assumed for tissue backscatter. Complex cepstrum has been used both for recovering the basic pulse and the reflection sequence. Power cepstrum is conventionally computed using FFT. Following new approaches have been suggested for its computation -

- (a) Adaptive Linear Prediction; and
- (b) Parameter Estimation.

These approaches, unlike FFT, assume a certain model for the signal. Thus they do not assume the signal to be zero or periodic outside the interval being studied.

#### Linear Prediction Techniques:

Adaptive linear prediction algorithms based on recently proposed escalator structure have been used for the deconvolution of the reflection sequence. These algorithms are adaptive escalator predictor (AEP) and adaptive least squares escalator predictor (ALSEP).

These are in general recursive techniques and can be effectively used for data whose characteristics are changing with time. The adaptive dynamics of these algorithms is disturbed when encountered with a delayed signal and the disturbance manifests itself as a large error in the output.

Adaptive escalator predictor is based on an escalator type structure whose weights are updated using a steepest descent method. Adaptive least squares escalator predictor uses Kalman filter equations to update its weights. Their respective performances have been studied as a function of the critical parameters involved and wide ranging SNRs. These studies have been carried out on both simulated and real data.

#### White Noise Estimator

This technique considers the deconvolution problem as a white noise estimation problem and is very much relevant to the present context as the occurrence of interfaces in a tissue is a random phenomenon having random coefficients. Since the technique assumes the state space representation of the observed signal, the input signal is first modelled in the state space using singular value decomposition procedure. The performance of the technique has been studied as a function of different orders of the input pulse, smoothing lags and SNRs.

The results obtained from the application of frequency domain techniques and homomorphic filtering show that these techniques in general are very sensitive to noise

and break down at SNRs as low as 25 db. In complex situations it has been observed that the reflection sequences obtained using homomorphic filtering especially, are beyond any meaningful analysis. Since these techniques involve the use of FFT at one stage or the other for their implementation, they can only be applied to stationary data. Also associated with the use of FFT are the basic assumptions that the data outside the interval being studied is either zero or periodic. These two conditions are rarely met. It has also been shown that the use of a window function for segmenting and smoothing the data has a lowpass filtering effect on it.

The use of later two techniques i.e. linear prediction and white noise estimator is intuitively justifiable as they are modelling based and are adaptive in nature. It has been shown that the linear prediction algorithms used in the present study are not very suitable for deconvolving the reflection sequences. This is because they are unable to adapt themselves to the changes occurring in the signal. It may be pointed out that these algorithms only model the signal as an autoregressive (AR) process, which largely explains their unsuitability to the present problem. The application of white noise estimator using suitable system

model has been shown to be very effective and insensitive to noise at low SNRs. This technique has been applied to both simulated and real data. The reflection sequences obtained from the real data show the occurrence of closely packed interfaces in the tissue.

#### Estimation of Propagation Velocity Using Unwrapped Phase Spectrum

Interest in the estimation of propagation velocity has grown from the fact that changes occurring in a tissue effects its composition and structure. This has a corresponding effect on the elastic modulus of the tissue. Since propagation velocity is a function of the elastic modulus of the medium, its value would naturally change with any changes occurring in the composition or the structure of the medium. Researchers in the past have reported the sensitivity of propagation velocity to the changes occurring in the tissue.

Propagation velocity in most of the techniques is computed by estimating the delay caused by the medium to the signal propagating through it. Very recently the use of unwrapped phase spectrum for the estimation of propagation velocity has been proposed. This technique compares the unwrapped phase spectra of the pulses which have propagated through the coupling medium with and without the specimen

being investigated. The results reported were for thick specimens. The present study has extended its application to tissues with small thickness. It has been shown that the technique is sensitive enough to measure propagation velocity in specimens of thickness of the order of 2.00 mm and its results are comparable to that of the pulse-transit-time method.

## CONTENTS

ACKNOWLEDGEMENT	iii
ABSTRACT	vii
CHAPTER I: REVIEW AND SCOPE OF THE THESIS	
Introduction	1
1.1 Ultrasound Tissue Interaction	2
1.2 Broad Overview	4
1.2.1. Estimation of Attenuation Coefficient Slope	4
1.2.2 Identification of Interfaces in the Tissue	7
1.2.3 Estimation of Propagation Velocity	23
REFERENCES	28
CHAPTER II: GENERATION AND SIMULATION OF TISSUE BACKSCATTERS AND OTHER ULTRASOUND SIGNALS	
Introduction	36
2.1 Generation and Recording of Ultrasound Signals	37
2.1.1 Instrumentation	37
2.1.2 Methodology	38
2.2 Modelling of Tissue Backscatter	44
2.2.1 Generation and Structure of Tissue Backscatter	44
2.2.2 Tissue Models	46
2.2.3 A Realistic Model for Tissue Backscatter	53
2.2.4 Corruption of Tissue Backscatters with White Gaussian Noise	59
2.3 Concluding Remarks	60
REFERENCES	61

CHAPTER III: ESTIMATION OF ATTENUATION COEFFICIENT SLOPE OF TISSUE USING BACKSCATTERED SIGNALS	
Introduction	62
3.1 Estimation of Attenuation Coefficient Slope Using Kuc's Technique	63
3.1.1 Distortion Modelling of Tissue Backscatter	66
3.1.2 A Discussion on Some Applica- tional Aspects of Estimation Algorithm	69
3.1.3 Investigation of Kuc's Technique Using Simulated Data	74
3.2 Estimation of Attenuation Coefficient Slope of Normal and Pathology Induced Pig Muscle Tissue in Vivo.	89
3.3 Concluding Remarks	98
REFERENCES	100
CHAPTER IV: SOME FREQUENCY DOMAIN TECHNIQUES FOR THE IDENTIFICATION OF INTERFACES IN THE TISSUE	
Introduction	102
4.1 Evaluation of Frequency Domain Deconvolution Techniques	104
4.1.1 Inverse Filtering	104
4.1.2 Wiener Filtering	106
4.1.3 Spectral Equalisation	107
4.2 Simulated Study	108
4.3 Concluding Remarks	117
REFERENCES	119

CHAPTER V : APPLICATION OF HOMOMORPHIC FILTERING AND  
RELATED ALGORITHMS TO TISSUE CHARACTERISATION

Introduction	120
5.1 Homomorphic Systems	121
5.1.1 A Canonical Representation of Homomorphic Systems	122
5.1.2 Characteristic System for Convolution	123
5.1.3 FFT Implementation of the Characteristic System	124
5.2 Application of Complex Cepstrum to Tissue Characterisation	124
5.2.1 Problems Involved in Complex Cepstrum Computation	127
5.2.2 Tissue Backscatter Experiments	137
5.3 Estimation of Reflection Sequence Using Power Cepstrum	148
5.3.1 Frequency Estimation of Sinusoids	155
5.3.2 Results	170
5.4 Concluding Remarks	173
REFERENCES	178

CHAPTER VI: IDENTIFICATION OF INTERFACES IN THE TISSUE  
USING ADAPTIVE LINEAR PREDICTION ALGORITHMS

Introduction	181
6.1 Criteria for the Comparison and Evaluation of Adaptive Algorithms	187
6.2 Input Orthogonalisation	189
6.3 Deconvolution of Tissue Backscatters Using Escalator Structure	192
6.3.1 Adaptive Escalator Predictor (AEP)-Gradient Search Algorithm	194
6.3.2 Adaptive Least Squares Escalator Predictor (ALSEP)-Least Squares Algorithm	197

6.3.3	Study of Convergence and Deconvolution Performance of the Escalator Based Algorithms Using Simulated Data	200
6.3.4	Study of Deconvolution Performance of the Algorithms Using Muscle Tissue Backscatter	220
6.3.5	Computational Requirements	220
6.4	Concluding Remarks	225
	REFERENCES	227

## CHAPTER VII: WHITE NOISE ESTIMATOR FOR ESTIMATION OF REFLECTION SEQUENCE

	Introduction	229
7.1	State Space Description of the System	231
7.2	Optimal 1-state White Noise Estimator	234
7.3	Study of Some of the Applicational Aspects of the White Noise Estimator Using Simulated Data	236
7.3.1	Optimal Choice of the Order of the System	236
7.3.2	Resolution Obtainable with the Estimator	237
7.3.3	Performance of the Estimator at Low SNRs	237
7.3.4	Criterion for the Size of the Smoothing Lag	238
7.4	A Segmental Model for White Noise Estimation	238
7.5	Estimation of Reflection Sequence from the Real Tissue Backscatter Using Segmental Model	251
7.6	Concluding Remarks	252
	REFERENCES	256

CHAPTER VIII:	ESTIMATION OF PROPAGATION VELOCITY IN TISSUES WITH SMALL THICKNESS USING UNWRAPPED PHASE	
	Introduction	257
8.1	Development of Propagation Velocity Estimation Technique Using Unwrapped Phase Spectrum	260
8.1.1	Formulation of the Estimation Algorithm	260
8.1.2	Implementational Aspects of the Estimator Technique	262
8.1.3	Calibration of the Estimat- ion Technique	264
8.2	Sensitivity of Technique Using Unwrapped Phase Spectrum for the Estimation of Propagation Velocity	265
8.2.1	Simulated Experiments	265
8.2.2	Real Experiments	266
8.2.3	Estimation of Propagation Velocity in Pig Skin	270
8.3	Concluding Remarks	273
	REFERENCES	274
CHAPTER IX	CONCLUSIONS	276